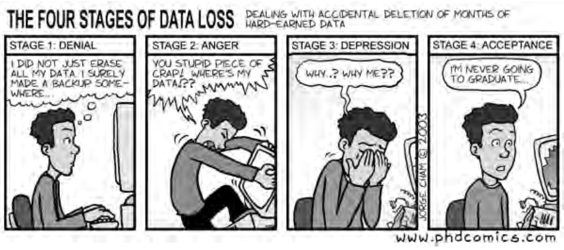
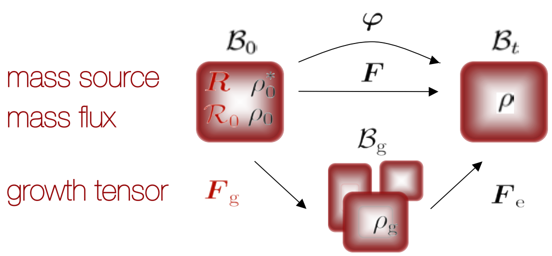
10 - finite element method - volume growth - implementation



day	date		topic
tue	jan	10	motivation - everything grows!
thu	jan	12	basics maths - notation and tensors
tue	jan	17	basic kinematics - large deformation and growth
thu	jan	19	kinematics - growing hearts
tue	jan	24	guest lecture - growing skin
thu	jan	26	guest lecture - growing leaflets
tue	jan	31	basic balance equations - closed and open systems
thu	feb	02	basic constitutive equations - growing tumors
tue	feb	07	volume growth - finite elements for growth
thu	feb	09	volume growth - growing arteries
tue	feb	14	volume growth - growing skin
thu	feb	16	volume growth - growing hearts
tue	feb	21	basic constitutive equations - growing bones
thu	feb	23	density growth - finite elements for growth
tue	feb	28	density growth - growing bones
thu	mar	01	everything grows! - midterm summary
tue	mar	06	midterm
thu	mar	08	remodeling - remodeling arteries and tendons
tue	mar	13	class project - discussion, presentation, evaluation
thu	mar	15	class project - discussion, presentation, evaluation
thu	mar	15	written part of final projects due

kinematics of finite growth

$$\boldsymbol{F} = \boldsymbol{F}_{\rm e} \cdot \boldsymbol{F}_{\rm g}$$

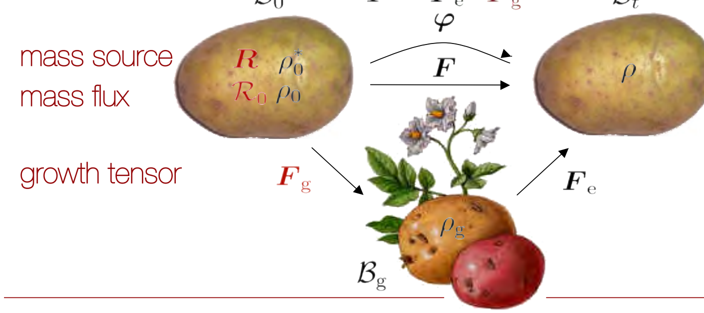


multiplicative decomposition

lee [1969], simo [1992], rodriguez, hoger & mc culloch [1994], epstein & maugin [2000], humphrey [2002], ambrosi & mollica [2002], himpel, kuhl, menzel & steinmann [2005]

the potato equations - kinematics

$$\boldsymbol{F} = \boldsymbol{F}_{\rm e} \cdot \boldsymbol{F}_{\rm g}$$



multiplicative decomposition

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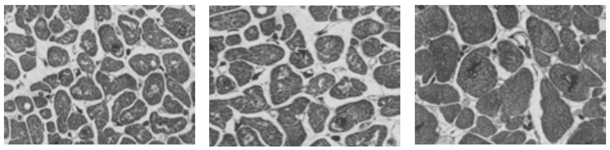
volume growth at constant density

- free energy $\psi_0 = \psi_0^{\text{neo}}(\boldsymbol{F}_{\text{e}})$
- stress $\boldsymbol{P}_{\text{e}} = \boldsymbol{P}_{\text{e}}^{\text{neo}}(\boldsymbol{F}_{\text{e}})$
- growth tensor $\boldsymbol{F}_{\text{g}} = \vartheta\, \boldsymbol{I}$ $\quad \mathrm{D}_t\vartheta = k_\vartheta(\vartheta)\; \mathrm{tr}(\boldsymbol{C}_{\text{e}} \cdot \boldsymbol{S}_{\text{e}})$

  growth function pressure
- mass source $\mathcal{R}_0 = 3\,\rho_0^* \vartheta^2 \mathrm{D}_t\vartheta$ increase in mass

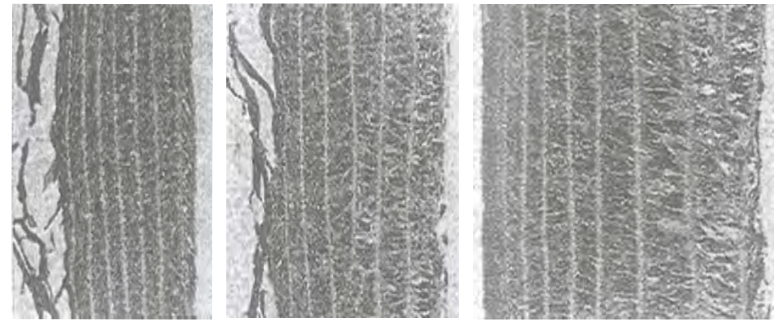


kinematic coupling of growth and deformation

rodriguez, hoger & mc culloch [1994], epstein & maugin [2000], humphrey [2002]

volume growth of the aortic wall

normosensitive hypersensitive severeley hypersensitive



wall thickening - thickening of musculoelastic fascicles

matsumoto & hayashi [1996], humphrey [2002]

compensatory wall thickening during atherosclerosis

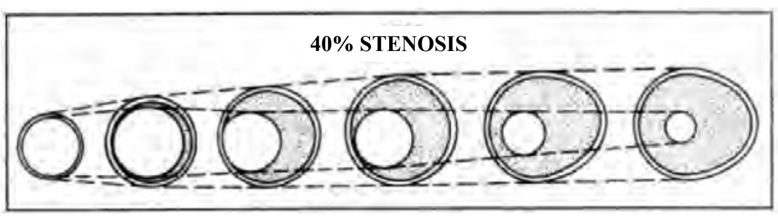
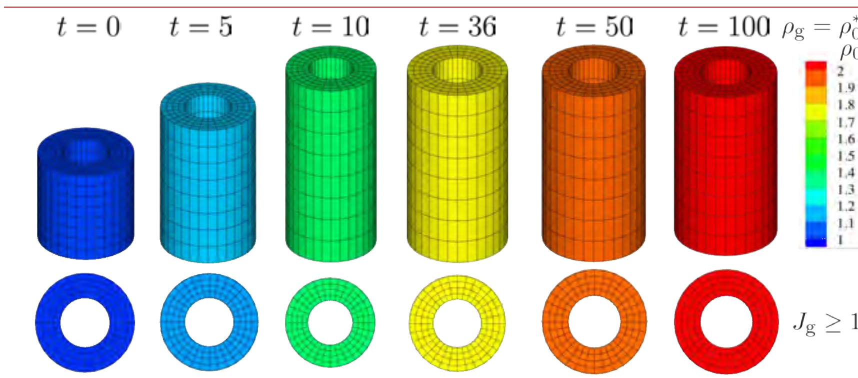


Figure 5. Diagrammic representation of a possible sequence of changes in atherosclerotic arteries leading eventually to lumen narrowing and consistent with the findings of this study. The artery enlarges initially (left to right in diagram) in association with the plaque accumulation to maintain an adequate, if not normal, lumen area. Early stages of lesion development may be associated with overcompensation. at more than 40% stenosis, however, the plaque area continues to increase to involve the entire circumference of the vessel, and the artery no longer enlarges at a rate suffcient to prevent the narrowing of the lumen.

glagov, weisenberg, zarins, stankunavicius, kolettis [1987]

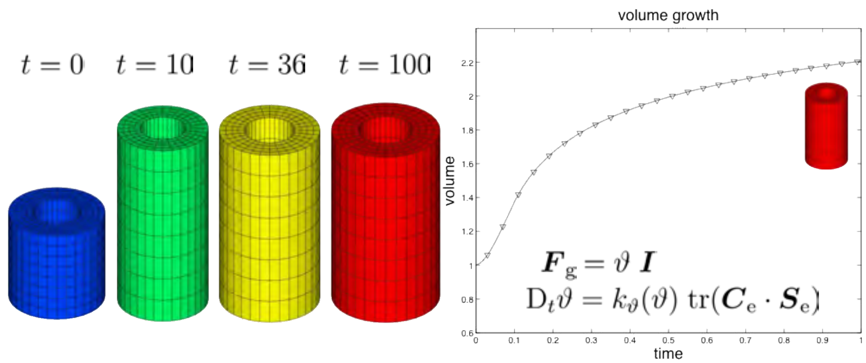
volume growth in cylindrical tube



stress-induced volume growth

himpel, kuhl, menzel & steinmann [2005]

volume growth in cylindrical tube

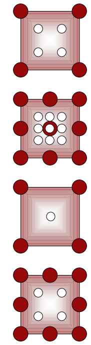


stress-induced volume growth

himpel, kuhl, menzel & steinmann [2005]

example - growth of aortic wall

integration point based solution of growth equation

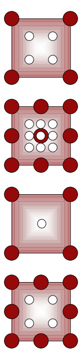


- loop over all time steps
  - global newton iteration
    - loop over all elements
      - loop over all quadrature points
        - local newton iteration to determine ϑ_{n+1}
      - determine element residual & partial derivative
    - determine global residual and iterational matrix
  - determine φ_{n+1}
- determine state of biological equilibrium

growth multiplier ϑ as internal variable

finite element method

integration point based solution of growth equation



loop over all time steps	nlin_fem
global newton iteration	nlin_fem
loop over all elements	brick3d
loop over all quadrature points	cnst_vol
local newton iteration ϑ_{n+1}	upd_vol
determine element residual & tangent	cnst_vol
determine global residual and tangent	brick3d
determine φ_{n+1}	nlin_fem
determine state of biological equilibrium	nlin_fem

growth multiplier ϑ as internal variable

finite element method

nlin_fem.m

```
%%% loop over all load steps %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
for is = (nsteps+1):(nsteps+inpstep);
   iter = 0;  residuum = 1;
%%% global newton-raphson iteration %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
   while residuum > tol
      iter=iter+1;
      R = zeros(ndof,1); K = sparse(ndof,ndof);
      e_spa = extr_dof(edof,dof);
%%%%% loop over all elements %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
      for ie = 1:nel
         [Ke,Re,Ie] = element1(e_mat(ie,:),e_spa(ie,:),i_var(ie,:),mat);
         [K, R, I ] = assm_sys(edof(ie,:),K,Ke,R,Re,I,Ie);
      end
%%%%% loop over all elements %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
      u_inc(:,2)=dt*u_pre(:,2);  R = R - time*F_pre;   dofold = dof;
      [dof,F] = solve_nr(K,R,dof,iter,u_inc);
      residuum= res_norm((dof-dofold),u_inc);
    end
%%% global newton-raphson iteration %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
    time = time + dt;   i_var = I;   plot_int(e_spa,i_var,nel,is);
end
%%% loop over all load steps %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```

finite element method

@ the element level

- determine global residual

check in matlab!

$$\mathbf{R}_J^{\varphi} = \mathbf{A}_{e=1}^{n_{\mathrm{el}}} \int_{\mathcal{B}_0^e} \nabla N_\varphi^j \cdot \boldsymbol{P}_{n+1} \mathrm{d}V$$

- residual of mechanical equilibrium/balance of momentum

righthand side vector for global system of equations

@ the element level

- stiffness matrix / iteration matrix

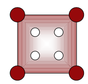
check in matlab!

$$\mathbf{K}_{JL}^{\varphi\varphi} = \frac{\partial \mathbf{R}_J^{\varphi}}{\partial \boldsymbol{\varphi}_L} = \mathbf{A}_{e=1}^{n_{\mathrm{el}}} \int_{\mathcal{B}_0^e} \nabla N_\varphi^j \cdot \mathrm{D}_F \boldsymbol{P} \cdot \nabla N_\varphi^l \mathrm{d}V$$

- linearization of residual wrt nodal dofs

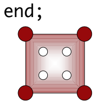
iteration matrix for global system of equations

quads_2d.m



```
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
function [Ke,Re,Ie]=element1(e_mat,e_spa,i_var,mat)
%%% element stiffness matrix Ke, residual Re, internal variables Ie %%%%
Ie = i_var;
Re = zeros(8,1);
Ke = zeros(8,8);
nod=4;            delta = eye(2);
indx=[1;3;5;7];  ex_mat=e_mat(indx);
indy=[2;4;6;8];  ey_mat=e_mat(indy);
%%% integration points %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
g1=0.577350269189626; w1=1;
gp(:,1)=[-g1; g1;-g1; g1];   w(:,1)=[ w1; w1; w1; w1];
gp(:,2)=[-g1;-g1; g1; g1];   w(:,2)=[ w1; w1; w1; w1];
wp=w(:,1).*w(:,2);      xsi=gp(:,1);      eta=gp(:,2);
%%% shape functions and derivatives in isoparametric space %%%%%%%%%%%%%
N(:,1)=(1-xsi).*(1-eta)/4;   N(:,2)=(1+xsi).*(1-eta)/4;
N(:,3)=(1+xsi).*(1+eta)/4;   N(:,4)=(1-xsi).*(1+eta)/4;
dNr(1:2:8  ,1)=-(1-eta)/4;   dNr(1:2:8  ,2)= (1-eta)/4;
dNr(1:2:8  ,3)= (1+eta)/4;   dNr(1:2:8  ,4)=-(1+eta)/4;
dNr(2:2:8+1,1)=-(1-xsi)/4;   dNr(2:2:8+1,2)=-(1+xsi)/4;
dNr(2:2:8+1,3)= (1+xsi)/4;   dNr(2:2:8+1,4)= (1-xsi)/4;
JT=dNr*[ex_mat;ey_mat]';
%%% element stiffness matrix Ke, residual Re, internal variables Ie %%%%
```

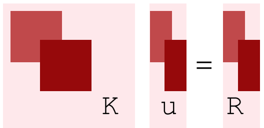

quads_2d.m



```
%%% loop over all integration points %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
for ip=1:4
indx=[2*ip-1; 2*ip];  detJ=det(JT(indx,:));
if detJ<10*eps;  disp('Jacobi determinant less than zero!');  end;
JTinv=inv(JT(indx,:));  dNx=JTinv*dNr(indx,:);
F=zeros(2,2);
for j=1:4
   jndx=[2*j-1; 2*j];
   F=F+e_spa(jndx)'*dNx(:,j)';
end
var = i_var(ip);
[A,P,var]=cnst_law(F,var,mat);
Ie(ip) = var;
for i=1:nod
   en=(i-1)*2;
   Re(en+ 1) =  Re(en+ 1) +(P(1,1)*dNx(1,i)' ...
                          + P(1,2)*dNx(2,i)') * detJ * wp(ip);
   Re(en+ 2) =  Re(en+ 2) +(P(2,1)*dNx(1,i)' ...
                          + P(2,2)*dNx(2,i)') * detJ * wp(ip);
end
%%% loop over all integration points %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%% element stiffness matrix Ke, residual Re, internal variables Ie %%%
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```

assm_sys.m

```
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
function [K,R,I]=assm_sys(edof,K,Ke,R,Re,I,Ie)
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%% assemble local element contributions to global tangent & residual %
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%% input:  edof  = [ elem X1 Y1 X2 Y2 ]    ... incidence matrix
%%%         Ke    = [ nedof x nedof ]       ... element tangent Ke
%%%         Re    = [ fx_1 fy_1 fx_2 fy_2 ] ... element residual Re
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%% output: K     = [ ndof x ndof ]         ... global tangent K
%%%         R     = [ ndof x 1 ]            ... global residual R
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
[nie,n]=size(edof);
I(edof(:,1),:)=Ie(:);
t=edof(:,2:n);
for i = 1:nie
   K(t(i,:),t(i,:)) = K(t(i,:),t(i,:))+Ke;
   R(t(i,:))        =R(t(i,:))       +Re;
end
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```



@ the integration point level

- constitutive equations - given $\boldsymbol{F}$ calculate $\boldsymbol{P}$

check in matlab!

$$\boldsymbol{P}(\boldsymbol{F}^{\mathrm{e}}) = \mu\,\boldsymbol{F}^{\mathrm{e}} + [\,\lambda\,\ln(\det(\boldsymbol{F}^{\mathrm{e}})) - \mu\,]\,\boldsymbol{F}^{\mathrm{e}\,-\,\mathrm{t}}$$

- stress calculation @ integration point level

stress for righthand side vector

@ the integration point level

- tangent operator / constitutive moduli

check in matlab!

$$\mathsf{A} = \frac{\mathrm{d}\boldsymbol{P}}{\mathrm{d}\boldsymbol{F}} = \frac{\partial \boldsymbol{P}}{\partial \boldsymbol{F}}\bigg|_{\boldsymbol{F}^{\mathrm{g}}} + \frac{\partial \boldsymbol{P}}{\partial \boldsymbol{F}^{\mathrm{g}}} : \frac{\partial \boldsymbol{F}^{\mathrm{g}}}{\partial \vartheta} \otimes \frac{\partial \vartheta}{\partial \boldsymbol{F}}\bigg|_{\boldsymbol{F}}$$

- linearization of stress wrt deformation gradient

tangents for iteration matrix

cnst_vol.m

```
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
function[A,P,var]=cnst_vol(F,var,mat,ndim)
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
determine tangent, stress and internal variable
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
emod = mat(1);   nue = mat(2);  kt = mat(3);  kc = mat(4);
mt   = mat(5);   mc  = mat(6);  tt = mat(7);  tc = mat(8); dt=mat(9);
xmu = emod / 2 / (1+nue);       xlm= emod * nue / (1+nue) /(1-2*nue);
%%% update internal variable%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
[var,ten1,ten2]=updt_vol(F,var,mat,ndim);
theta =var(1)+1; Fe=F/theta;Fe_inv=inv(Fe);Je=det(Fe);delta=eye(ndim);
%%% first piola kirchhoff stress %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
P = xmu * Fe + (xlm * log(Je) - xmu) * Fe_inv';
%%% tangent %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
for i=1:ndim; for j=1:ndim; for k=1:ndim; for l=1:ndim
    A(i,j,k,l) =  xlm * Fe_inv(j,i)*Fe_inv(l,k) ...
               - (xlm * log(Je) - xmu) * Fe_inv(l,i)*Fe_inv(j,k) ...
               +                 xmu  *  delta(i,k)* delta(j,l) ...
               +                          ten1(i,j)*  ten2(k,l);
end, end, end, end;
A = A / theta;
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```

@ integration point level

- discrete update of growth multiplier

check in matlab!

$$R^{\vartheta}_{n+1} = \vartheta_{n+1} - \vartheta_n - k\,\mathrm{tr}(\boldsymbol{M}^{e})\,\Delta t$$

- residual of biological equilibrium

local newton iteration

updt_vol.m

```
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%% local newton-raphson iteration %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
while abs(res) > tol
  iter=iter+1;
  Fe = F/the_k1; Fe_inv = inv(Fe);   Ce = Fe'*Fe; Ce_inv = inv(Ce);
  Je = det(Fe);  delta  = eye(ndim);
  Se = xmu * delta + (xlm * log(Je) - xmu) * Ce_inv;
  Me = Ce*Se;       tr_Me = trace(Me);
  CeLeCe = ndim * ndim * xlm - 2 * ndim * (xlm * log(Je) - xmu);
  dtrM_dthe = - 1/the_k1 * ( 2*tr_Me + CeLeCe );
  if tr_Me > 0
     k       = kt*((tt-the_k1)/(tt-1))^mt;
     dk_dthe = k  /(the_k1-tt)        *mt;
  else
     k       = kc*((the_k1-tc)/(1-tc))^mc;
     dk_dthe = k  /(the_k1-tc)        *mc;
  end
res  = k * tr_Me * dt - the_k1 + the_k0;
dres =(dk_dthe * tr_Me + k * dtrM_dthe)*dt -1;
the_k1 =  the_k1 -res/dres;
if(iter>20); disp(['*** NO LOCAL CONVERGENCE ***']); return; end;
%%% local newton-raphson iteration %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```

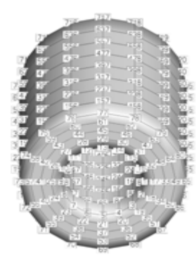

ex_tube1.m

```
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
function [q0,edof,emat,bc,F_ext,mat,ndim,nel,node,ndof,nip,nlod] = ex_tube1
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
%%% material parameters for volume growth %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
emod = 3.0; nue = 0.3;
kt   = 0.5; kc  = 0.25; mt = 4.0; mc = 5.0; tt = 1.5; tc = 0.5;dt=1.0;
mat=[emod,nue,kt,kc,mt,mc,tt,tc,dt];
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
l   =    2.0;       % length
ra  =    1.0;       % inner radius
ri  =    0.5;       % outer radius
nez =      8;       % number of elements in longitudinal direction
ner =      4;       % number of elements in radial direction
nep =     16;       % number of elements in circumferential direction
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
tol  = 1e-8;
ndim = 3;
nip  = 8;
nel = nez * ner * nep;
node= (nez+1)*(ner+1)*nep;
ndof = ndim*node;
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```


ex_tube1.m

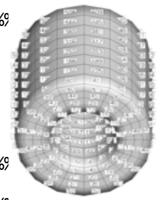
```
%%% coordinates %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
q0 = zeros(ndim*node,1);
nn = 0;

delta_z =       l / nez;
delta_r = (ra-ri) / ner;
delta_t =    2*pi / nep;
for iz = 0:nez
  z = iz * delta_z;
  for ir = 0:ner
    r = ri + ir * delta_r;
    for ip = 0:(nep-1)
      p = ip * delta_t;
      nn = nn +ndim;
      q0(nn-2,1) = r*cos(p);
      q0(nn-1,1) = r*sin(p);
      q0(nn   ,1) = z;
    end
  end
end
%%% coordinates %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```



ex_tube1.m

```
%%% connectivity %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
for ie = 1:nel
   edof(ie,:)=[ie, ndim*enod(ie,1)-2  ndim*enod(ie,1)-1  ndim*enod(ie,1) ...
                   ndim*enod(ie,2)-2  ndim*enod(ie,2)-1  ndim*enod(ie,2) ...
                   ndim*enod(ie,3)-2  ndim*enod(ie,3)-1  ndim*enod(ie,3) ...
                   ndim*enod(ie,4)-2  ndim*enod(ie,4)-1  ndim*enod(ie,4) ...
                   ndim*enod(ie,5)-2  ndim*enod(ie,5)-1  ndim*enod(ie,5) ...
                   ndim*enod(ie,6)-2  ndim*enod(ie,6)-1  ndim*enod(ie,6) ...
                   ndim*enod(ie,7)-2  ndim*enod(ie,7)-1  ndim*enod(ie,7) ...
                   ndim*enod(ie,8)-2  ndim*enod(ie,8)-1  ndim*enod(ie,8)];
end
%%% boundary conditions %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
du = l/2; nb = 0;
for ib = 1:(nep*(ner+1))
  if(abs(q0(ndim*(node-nep*(ner+1))+ndim*ib-2)-0.0)<tol)
    nb = nb+1;     bc(nb,:) = [ndim*ib-2  0];
  end  if(abs(q0(ndim*(node-nep*(ner+1))+ndim*ib-1)-0.0)<tol)
end
%%% loading %%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
load  = 0.0;F_ext = zeros(ndof,1);  nlod  = 1;
%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%%
```



ex_tube1.m

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Computational modelling of isotropic multiplicative growth

G. Himpel, E. Kuhl, A. Menzel, P. Steinmann

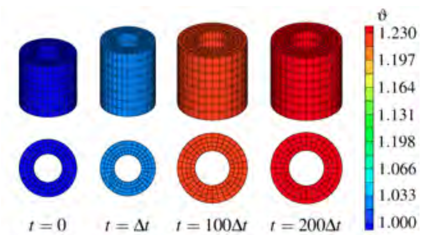


Figure 10 : Deformation of the tube and evolution of the stretch ratio for an axial stretch $u = 1.0$.

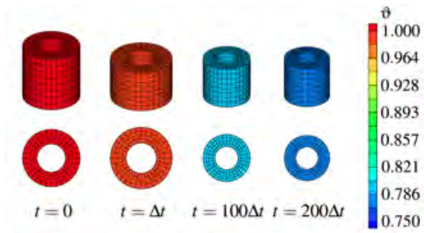
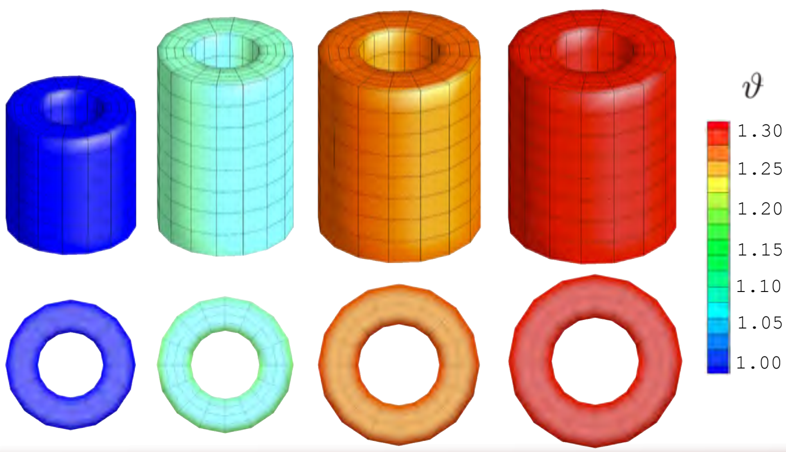


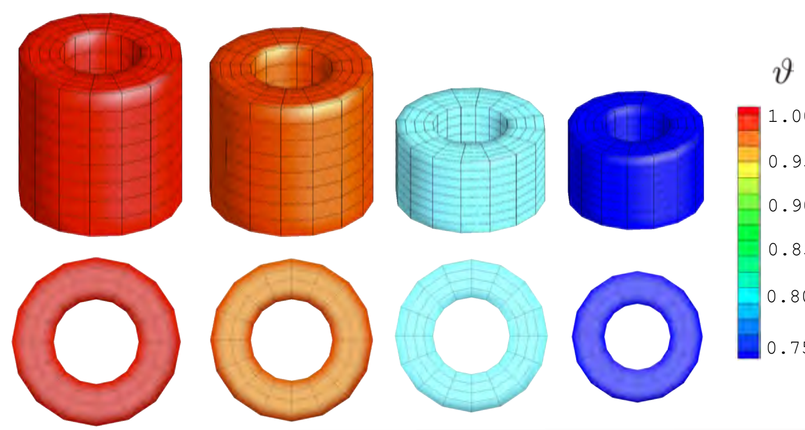
Figure 12 : Deformation of the tube and evolution of the stretch ratio for an axial compression $u = -1.0$.

himpel, kuhl, menzel & steinmann [2005]

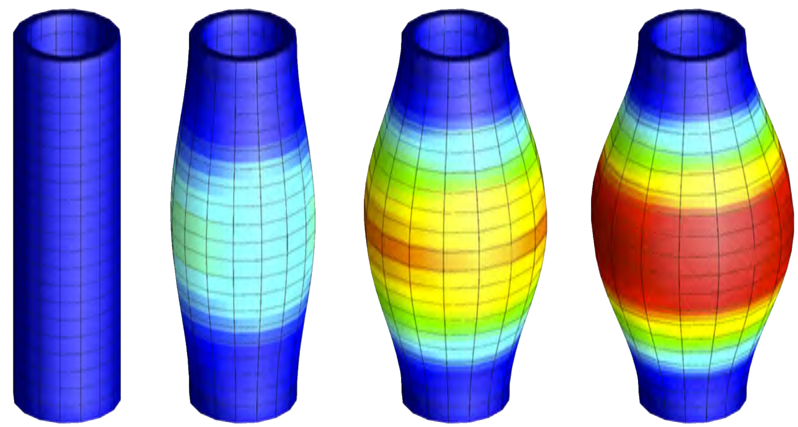
ex_tube1.m



ex_tube2.m



ex_tube3.m



finite element method

atherosclerosis

atherosclerosis is a condition in which an artery wall thickens as the result of a build-up of fatty materials. the atheromatous plaques, although compensated for by artery enlargement, eventually lead to plaque rupture and clots inside the arterial lumen. the clots leave behind stenosis, a narrowing of the artery, and insufficient blood supply to the tissues and organ it feeds. if the artery enlargement is excessive, a net aneurysm results. these complications of advanced atherosclerosis are chronic, slowly progressive and cumulative.

Wikipedia The Free Encyclopedia

example - atherosclerosis

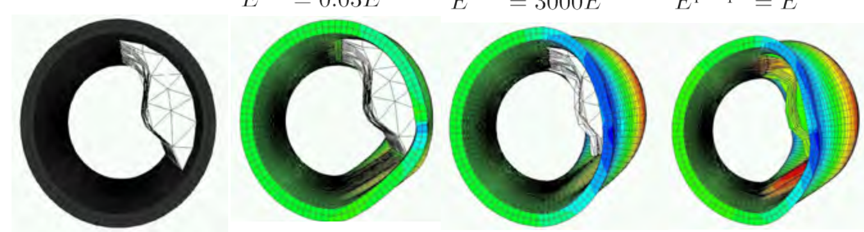
atherosclerosis

[greek] arteria = artery / sclerosis = hardening

example - atherosclerosis

qualitative simulation of atherosclerosis

initial conditions | adiposis $E^{\text{fat}} = 0.03 E^{\text{tissue}}$ | calcification $E^{\text{lime}} = 3000 E^{\text{tissue}}$ | growing plaque $E^{\text{plaque}} = E^{\text{tissue}}$



early stage
soft plaque pressed into wall

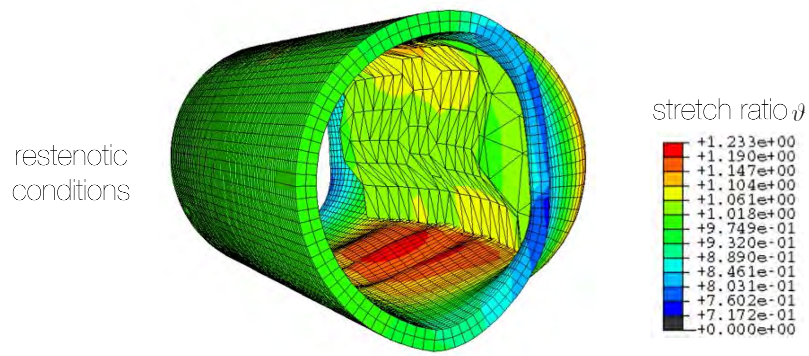
later stage
stiff plaque induces high stresses

overall thickening - thickening of individual fascicles

holzapfel [2001], holzapfel & ogden [2003], kuhl, maas, himpel & menzel [2007]

example - atherosclerosis

qualitative simulation of atherosclerosis



re-nerrowing of x-section in response to high stress

kuhl, maas, himpel & menzel [2007]

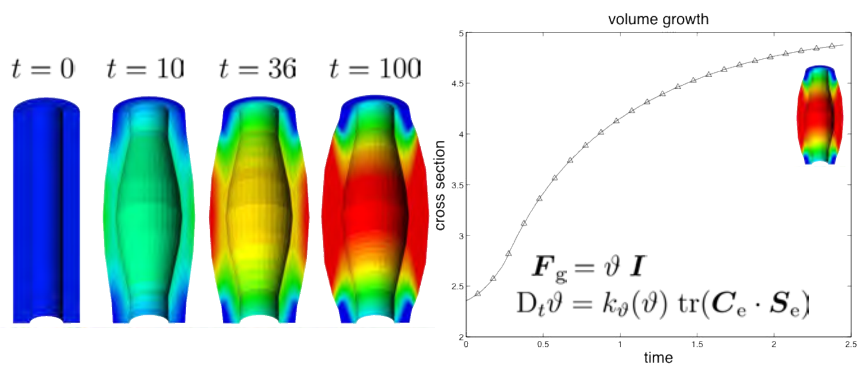
example - atherosclerosis 33

in-stent restenosis

restenosis is the reoccurrence of stenosis, the narrowing of a blood vessel, leading to restricted blood flow. restenosis usually pertains to a blood vessel that has become narrowed, received treatment, and subsequently became renarrowed. in some cases, surgical procedures to widen blood vessels can cause further narrowing. during balloon angioplasty, the balloon 'smashes' the plaques against the arterial wall to widen the size of the lumen. however, this damages the wall which re-sponds by using physiological mechanisms to repair the damage and the wall thickens.

example - stenting and restenosis 34

qualitative simulation of stent implantation

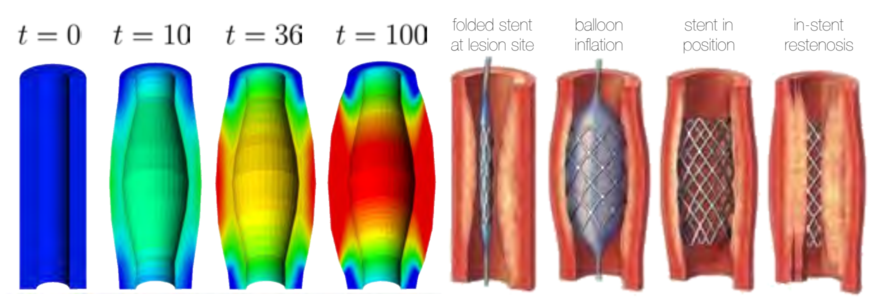


stress-induced volume growth

kuhl, maas, himpel & menzel [2007]

example - stenting and restenosis 35

qualitative simulation of stent implantation



stress-induced volume growth

kuhl, maas, himpel & menzel [2007]

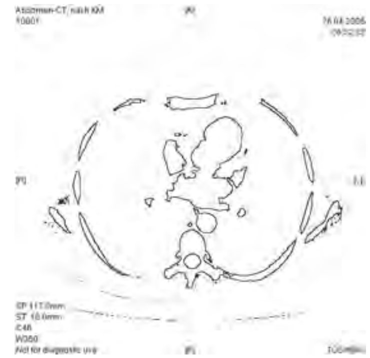
example - stenting and restenosis 36

generation of patient specific model

computer tomography - typical cross section

kuhl, maas, himpel & menzel [2007]

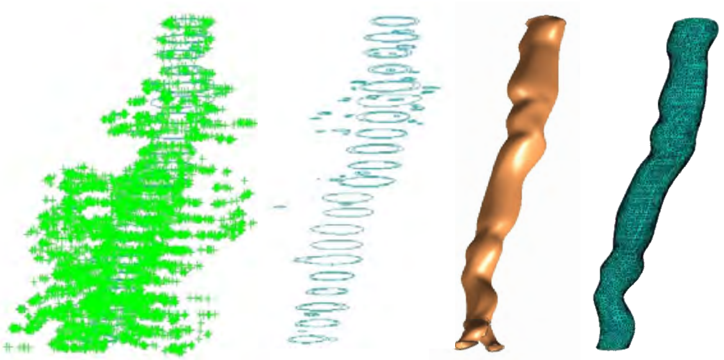
generation of patient specific model



outline of ct image - typical cross section

kuhl, maas, himpel & menzel [2007]

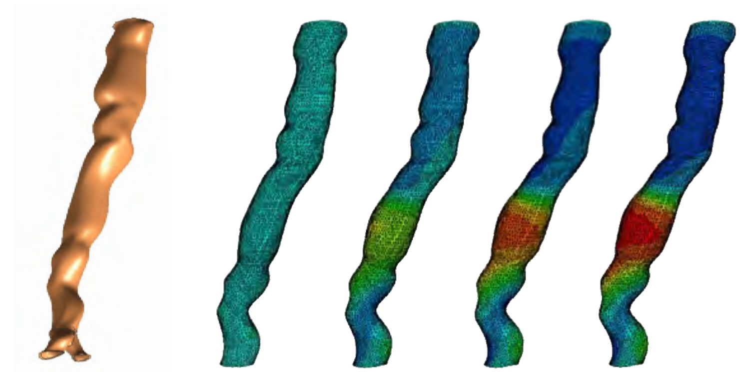
generation of patient specific model



from computer tomography to finite element model

kuhl, maas, himpel & menzel [2007]

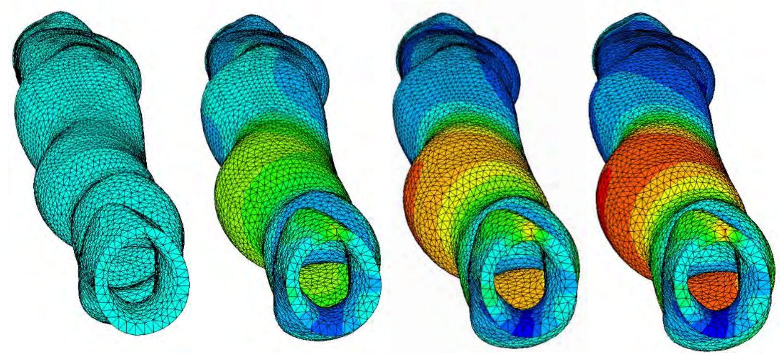
virtual stent implantation - patient specific model



tissue growth - response to virtual stent implantation

kuhl, maas, himpel & menzel [2007]

virtual stent implantation - patient specific model



tissue growth - response to virtual stent implantation

kuhl, maas, himpel & menzel [2007]

example - stenting and restenosis