

17 - examples - remodeling



17 - examples

1

growth, remodeling and morphogenesis

growth [groʊθ] which is defined as added mass, can occur through cell division (hyperplasia), cell enlargement (hypertrophy), secretion of extracellular matrix, or accretion @ external or internal surfaces. negative growth (atrophy) can occur through cell death, cell shrinkage, or resorption. in most cases, hyperplasia and hypertrophy are mutually exclusive processes. depending on the age of the organism and the type of tissue, one of these two growth processes dominates.

Taber „Biomechanics of growth, remodeling and morphogenesis“ [1995]



remodeling

2

growth, remodeling and morphogenesis

remodeling [ri'mad.lɪŋ] involves changes in material properties. These changes, which often are adaptive, may be brought about by alterations in modulus, internal structure, strength, or density. for example, bones, and heart muscle may change their internal structures through reorientation of trabeculae and muscle fibers, respectively.

Taber „Biomechanics of growth, remodeling and morphogenesis“ [1995]



remodeling

3

growth, remodeling and morphogenesis

morphogenesis [mɔːr.fɒ'dʒen.ə.sɪs] is the generation of animal form. usually, the term refers to embryonic development, but wound healing and organ regeneration are also morphogenetic events. morphogenesis contains a complex series of stages, each of which depends on the previous stage. during these stages, genetic and environmental factors guide the spatial-temporal motions and differentiation (specification) of cells. a flaw in any one stage may lead to structural defects.

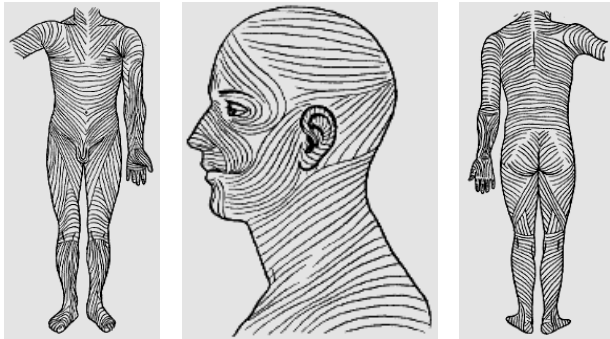
Taber „Biomechanics of growth, remodeling and morphogenesis“ [1995]



remodeling

4

langer's lines - anisotropy of human skin



lines of tension - orientation of collagen fiber bundles

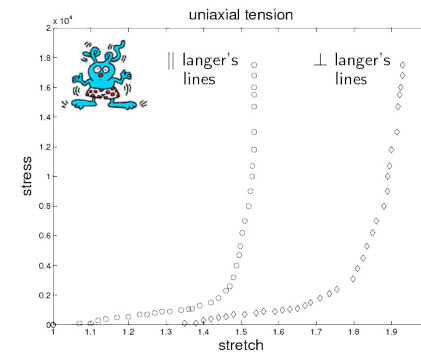
Carl Ritter von Langer [1819-1887]



remodeling

5

langer's lines - anisotropy of rabbit skin



stiffer || to langer's lines - stress locking @crit stretch

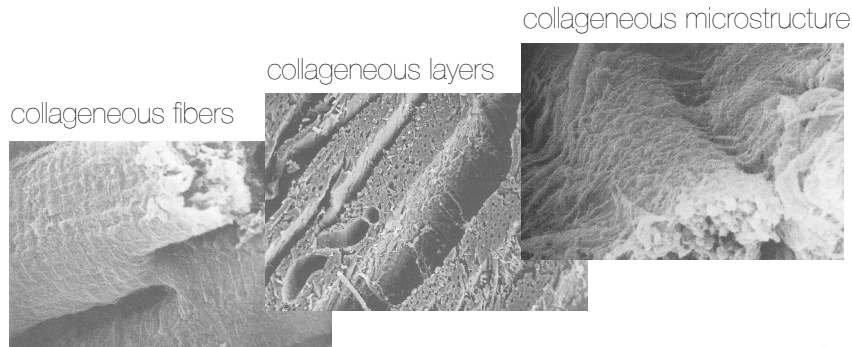
Lanir & Fung [1974]



remodeling

6

collagen fibers - anisotropy of human tissue



directional strengthening due to collagen fibers

Humphrey [2002]



remodeling

7

collagen fibers - anisotropy of human tissue



directional strengthening due to collagen fibers

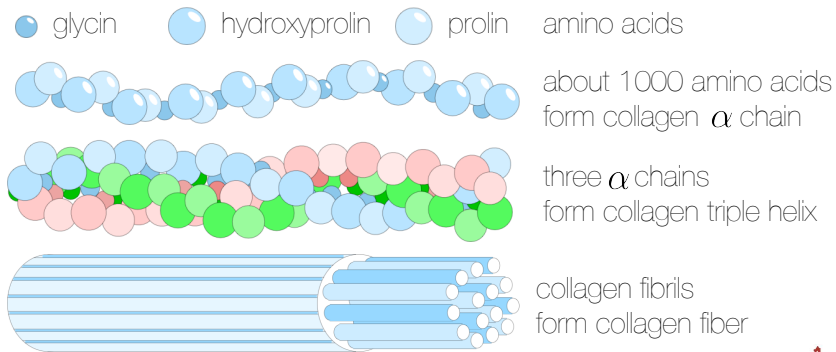
Vidik [1973]



remodeling

8

collagen fibers - hierarchical microstructure

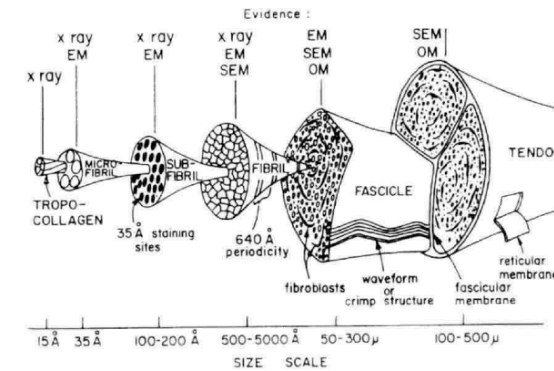


directional strengthening due to collagen fibers

remodeling

9

fundamental idea - hierarchical model



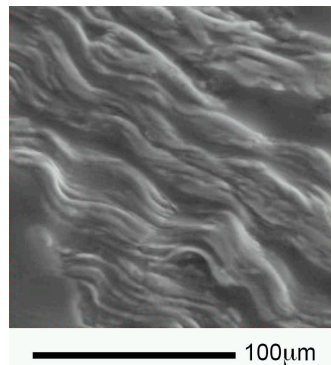
limited set of parameters - clear physical interpretation

Galeski & Baer [1978]

remodeling

10

fundamental idea - hierarchical model



hypotheses

- I biological tissues seek to restore stress @homeostatic value
- II collagen fibers as main load carrying constituents adapt orientation to minimize stress
- III collagen fiber remodeling can be modeled phenomenologically to provide further insight into tissue's microstructure

collagen fibers in adventitia of human aorta

Holzapfel [2005]

remodeling

11

- I micromechanics • collagen chain
- II macromechanics • chain network
- III biomechanics • tissue remodeling

remodeling

12

statistical mechanics of long chain molecules



entropic elasticity - entropy increases upon stretching

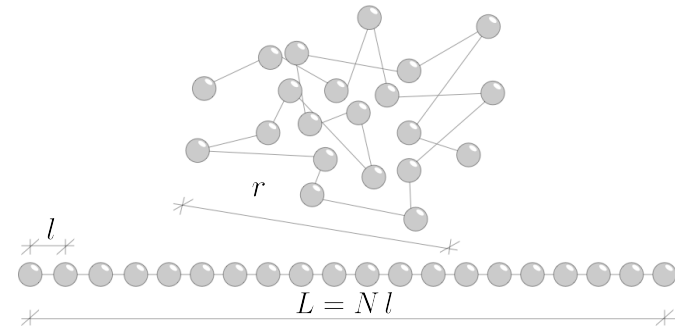
Kuhn [1936], [1938], Porod [1949], Kratky & Porod [1949], Treolar [1958], Flory [1969], Bustamante, Smith, Marko & Siggia [1994], Marko & Siggia [1995], Rief [1997], Holzapfel [2000], Bischoff, Arruda & Gosh [2000], [2002], Ogden, Saccamandi & Sgura [2006]



remodeling - micromechanics

13

uncorrelated freely jointed chain



$$\psi^{fjc} = k \theta N \left[\frac{r}{L} \mathcal{L}^{-1} + \ln \left(\frac{\mathcal{L}^{-1}}{\sinh(\mathcal{L}^{-1})} \right) \right]$$

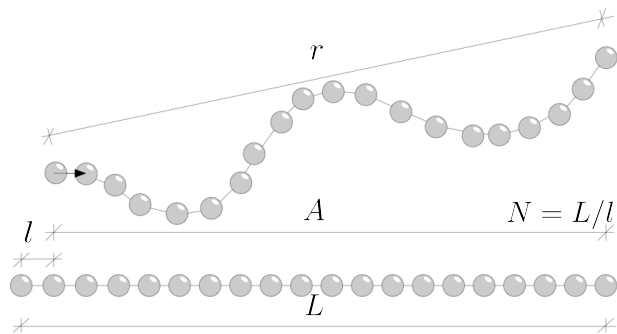
micromechanically motivated parameter - contour length L



remodeling - micromechanics

14

correlated wormlike chain



$$\psi^{wlc} = \frac{k \theta L}{4 A} \left[2 \frac{r^2}{L^2} + \frac{1}{[1 - r/L]} - \frac{r}{L} \right]$$

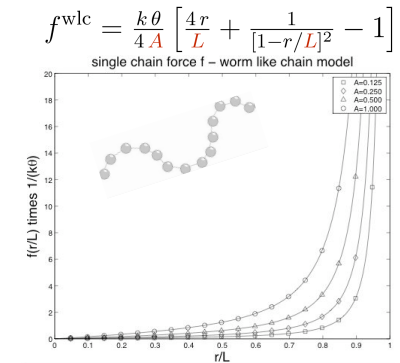
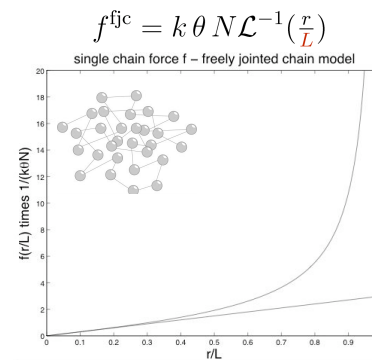
micromechanically motivated parameters - contour length L and persistence length A



remodeling - micromechanics

15

constitutive equations - collagen chain



characteristic locking behavior - initial stiffness of wlc

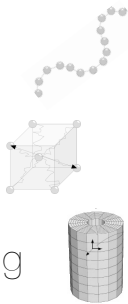
micromechanically motivated parameters - contour length L and persistence length A



remodeling - micromechanics

16

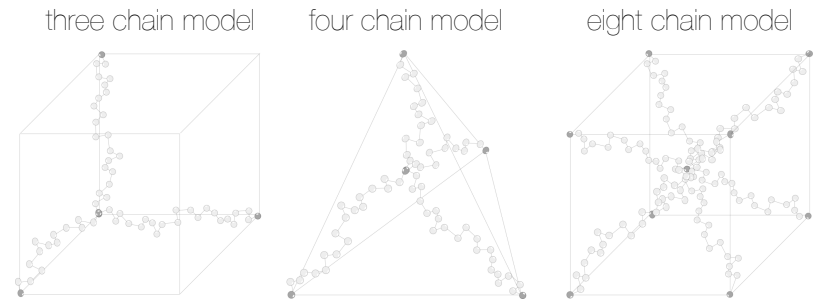
- I micromechanics • collagen chain
- II macromechanics • chain network
- III biomechanics • tissue remodeling



remodeling

17

concept of chain network models



representative isotropic network of cross-linked chains

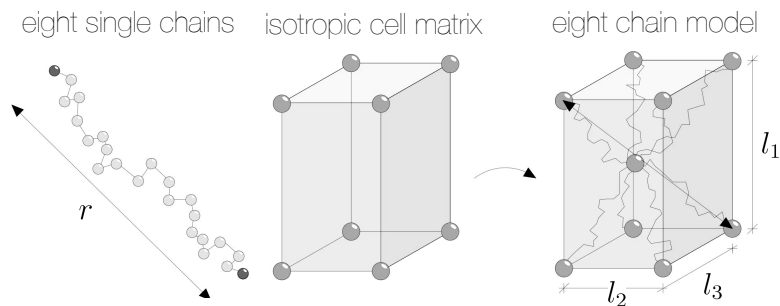
Flory & Rehner [1943], James & Guth [1943], Wang & Guth [1952], Treloar [1958], Arruda & Boyce [1993], Wu & van der Giessen [1993], Boyce [1996], Boyce & Arruda [2000], Bischoff, Arruda & Groh [2002], Miehe, Göktepe & Lulei [2004]



remodeling - macromechanics

18

constitutive equations - chain network



$$\Psi^{\text{chn}} = \frac{1}{8} \gamma^{\text{chn}} \sum_{i=1}^8 \psi^{\text{wlc}}(r) \quad \text{with} \quad r = r(\mathbf{F})$$

$$\Psi^{\text{iso}} = \frac{1}{2} \lambda \ln^2(\det(\mathbf{F})) + \frac{1}{2} \mu [\mathbf{F}^t : \mathbf{F} - n^{\text{dim}} - 2 \ln(\det(\mathbf{F}))]$$

micromechanically motivated parameters - chain density γ^{chn} and cell dimensions l_1, l_2, l_3

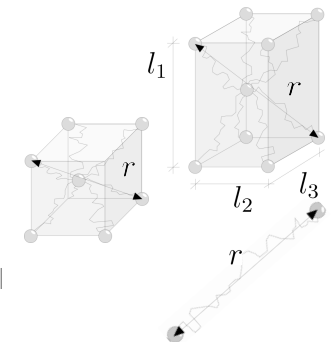


remodeling - macromechanics

19

orthotropic chain network model

- general case **orthotropic** network model
 $l_1 \neq l_2 \neq l_3 \quad r = \sqrt{l_1^2 \bar{I}_1^C}$
- special case **isotropic** network model
 $l_1 = l_2 = l_3 = l \quad r = l \sqrt{\bar{I}_1^C}$
- special case **transversely isotropic** model
 $l_2 = l_3 = 0 \quad r = l_1 \sqrt{\bar{I}_1^C}$



traditional arruda boyce model as special case

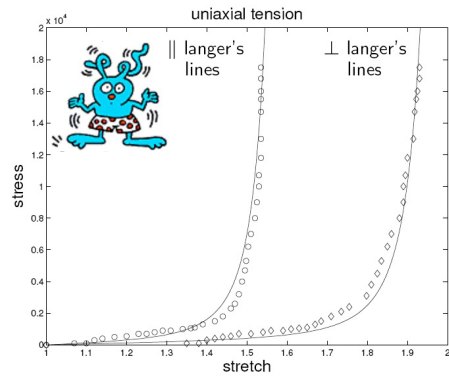
invariants $I_1^C = \mathbf{C} : \mathbf{I}$ and $\bar{I}_1^C = \mathbf{n}_l \cdot \mathbf{C} \cdot \mathbf{n}_l$



remodeling - macromechanics

20

experiment vs simulation - rabbit skin



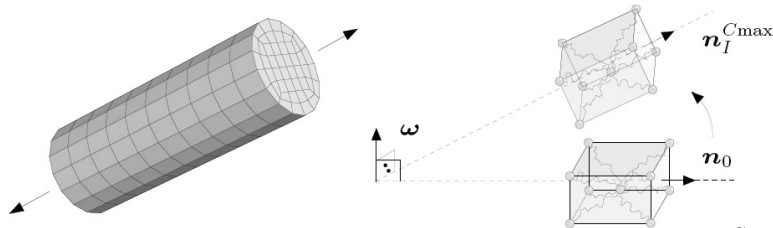
stiffer || to langer's lines - stress locking @crit stretch

Lanir & Fung [1974], Kuhl, Garikipati, Arruda & Grosch [2005]

example - rabbit skin

21

adaptation of microstructural direction



- gradual alignment of fiber direction \mathbf{n}_0 with max principal strain $\mathbf{n}_I^{C_{\max}}$

$$\mathbf{n}_0 \rightarrow \mathbf{n}_I^{C_{\max}} \quad \mathbf{C} = \lambda_I^C \mathbf{n}_I^C \otimes \mathbf{n}_I^C$$

- exponential update/euler-rodriques for direction of transverse isotropy \mathbf{n}_0

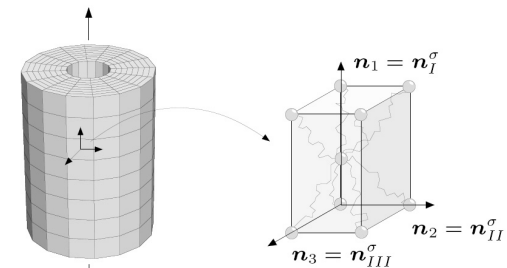
$$\mathbf{n}_0^{k+1} = \exp(-\Delta t \mathbf{e}^3 \cdot \boldsymbol{\omega}) \cdot \mathbf{n}_0^k \quad \boldsymbol{\omega} = [\mathbf{n}_0^k \times \mathbf{n}_I^{C_{\max}}] / \kappa_{\boldsymbol{\omega}}$$

Fyrhje & Carter [1986], Cowin [1989], [1994], Vianello [1996], Sgarra & Vianello [1997], Menzel [2004], Driessen [2006], Kuhl, Menzel & Garikipati [2006]

remodeling - biomechanics

23

adaptation of microstructural axes



- instantaneous alignment of microstructure \mathbf{n}_I wrt eigenvectors \mathbf{n}_I^{σ}

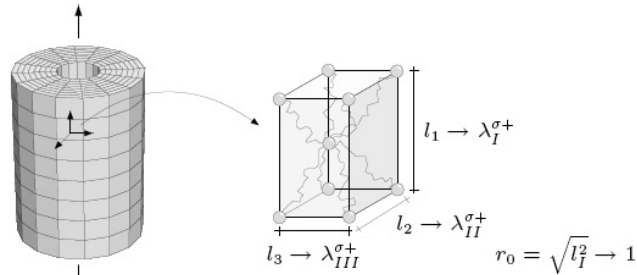
$$\mathbf{n}_I \doteq \mathbf{n}_I^{\sigma} \quad \boldsymbol{\sigma} = \lambda_I^{\sigma} \mathbf{n}_I^{\sigma} \otimes \mathbf{n}_I^{\sigma}$$

„the unit cell used in each of the network models is taken to deform in principal stretch space.“ Boyce & Arruda [2000]

remodeling - biomechanics

24

adaptation of fiber dimensions



- gradual adaptation of microstructural dimensions l_I wrt eigenvalues⁺ $\lambda_I^{\sigma+}$
- $$l_I \rightarrow \begin{cases} \lambda_I^{\sigma+} / \|\lambda_I^{\sigma+}\| & \text{if } \lambda_I^{\sigma} > 0 \\ 0 & \text{if } \lambda_I^{\sigma} \leq 0 \end{cases} \quad \sigma = \lambda_I^{\sigma} \mathbf{n}_I^{\sigma} \otimes \mathbf{n}_I^{\sigma}$$

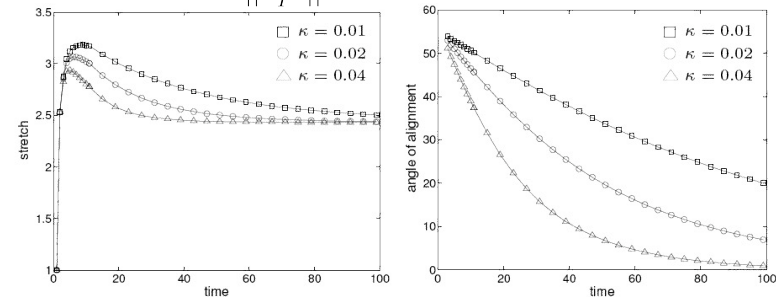
"the collagen fibers are located between the directions of the maximum principal stresses." Hariton, de Botton, Gasser & Holzapfel [2006]

remodeling - biomechanics

25

remodeling of collagen fibers - uniaxial tension

$$l_I = \left[\frac{\lambda_I^{\sigma+}}{\|\lambda_I^{\sigma+}\|} - l_I^0 \right] [1 - \exp(-\kappa t)] + l_I^0$$



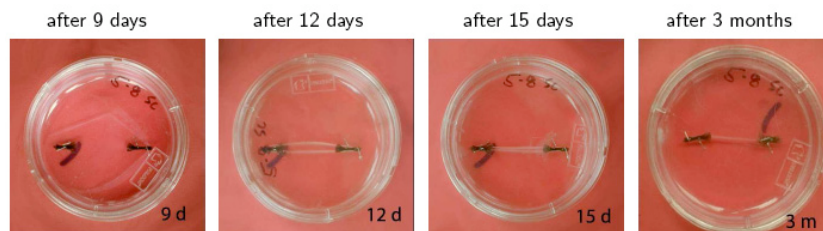
stress driven adaptation of microstructure

micromechanically motivated parameter κ

remodeling - biomechanics

26

remodeling of collagen fibers - living tendon



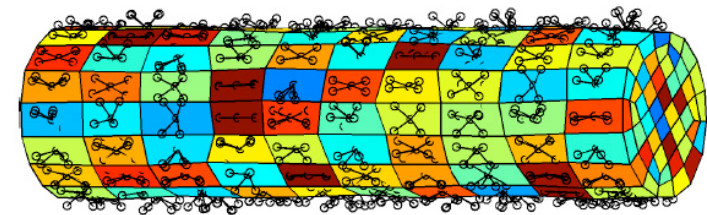
- ex vivo engineered tendon shows characteristics of embryonic tendon
- remodeling of collagen fibers upon mechanical loading
- long term goal mechanically stimulated tissue engineering

Calve, Dennis, Kosnik, Baar, Grosh & Arruda [2004]

example - tissue engineering

27

remodeling of collagen fibers - living tendon



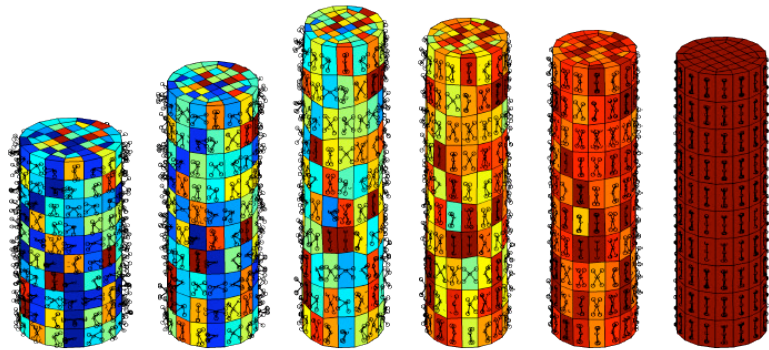
- finite element simulation of functional adaptation in tendons
- wormlike chain model with initial random anisotropy
- analysis of fiber reorientation in uniaxial tension

Kuhl, Garikipati, Arruda & Grosh [2005]

example - tissue engineering

28

remodeling of collagen fibers - living tendon

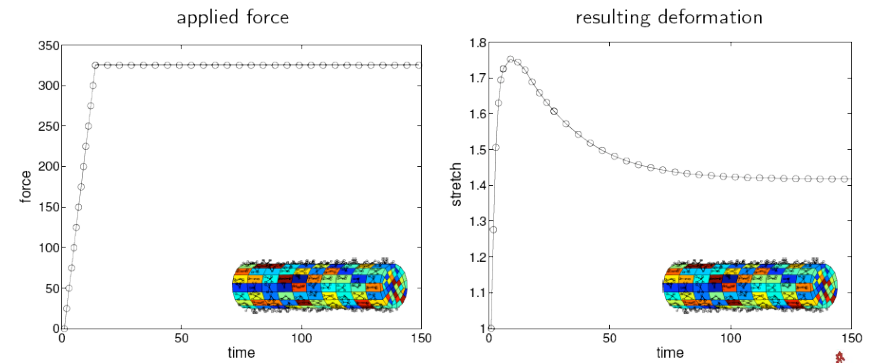


gradual fiber alignment with max principal stress



example - tissue engineering

remodeling of collagen fibers - living tendon

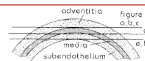
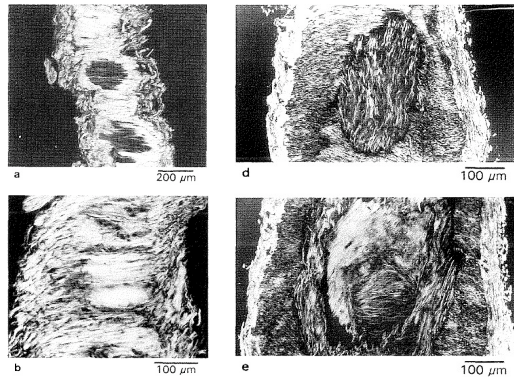


characteristic locking, remodeling & stiffening



example - tissue engineering

tangentially sectioned brain arteries



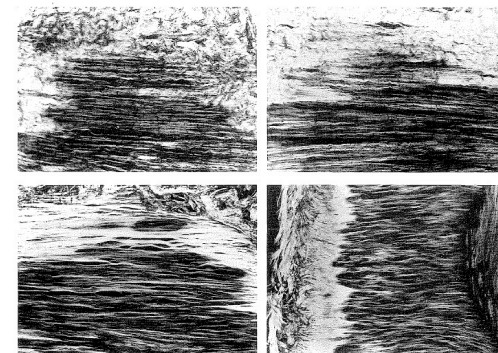
circularly polarized light micrographs

Finlay [1995]



example - arterial wall

tangentially sectioned brain arteries



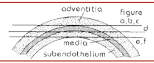
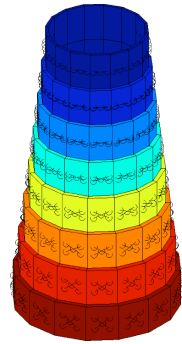
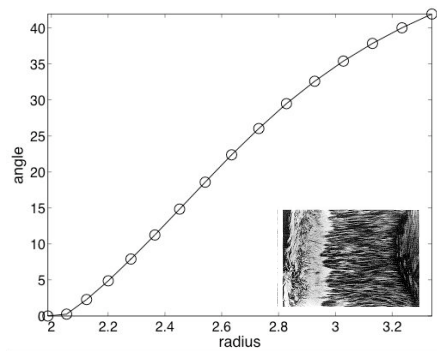
circularly polarized light micrographs

Finlay [1995]



example - arterial wall

remodeling of collagen fibers



stress driven functional adaptation

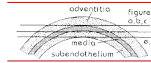
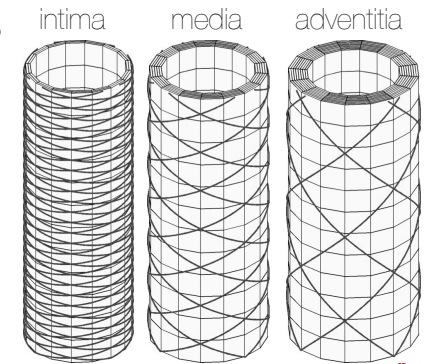
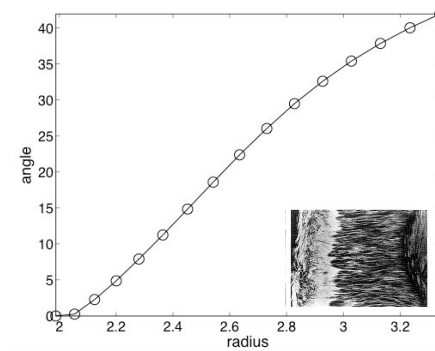
Kuhl & Holzapfel [2007]



example - arterial wall

33

remodeling of collagen fibers



stress driven functional adaptation

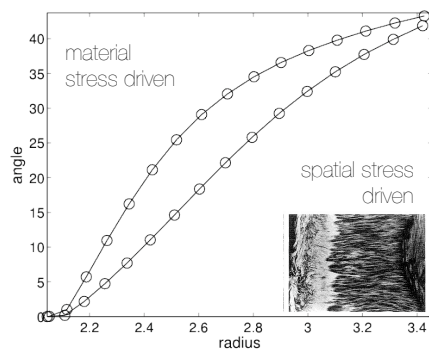
Kuhl & Holzapfel [2007]



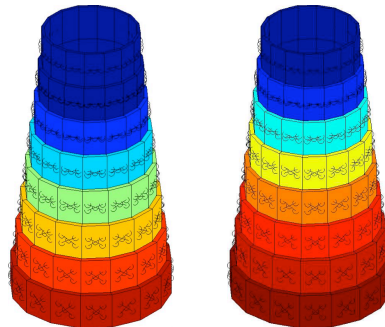
example - arterial wall

34

sensitivity wrt driving force - spatial vs material stress



$$\sigma = \lambda_1^\sigma \mathbf{n}_1^\sigma \otimes \mathbf{n}_1^\sigma \quad \mathbf{S} = \lambda_1^S \mathbf{n}_1^S \otimes \mathbf{n}_1^S$$



true spatial driving force more reasonable

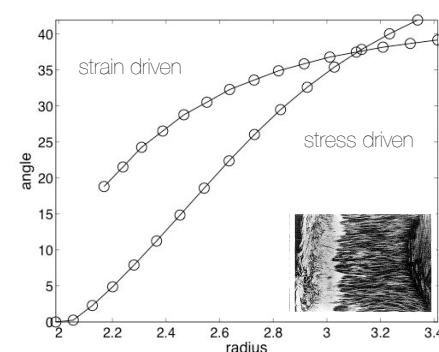
Kuhl & Holzapfel [2007]



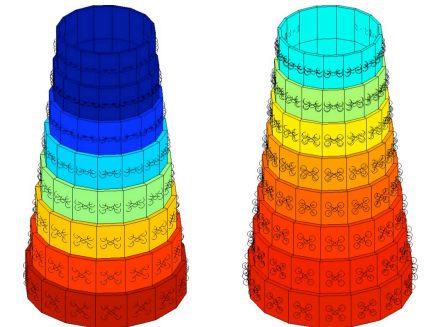
example - arterial wall

35

sensitivity wrt driving force - stress vs strain



$$\sigma = \lambda_1^\sigma \mathbf{n}_1^\sigma \otimes \mathbf{n}_1^\sigma \quad \mathbf{b} = \lambda_1^b \mathbf{n}_1^b \otimes \mathbf{n}_1^b$$



eigenvectors coincide but eigenvalues differ significantly

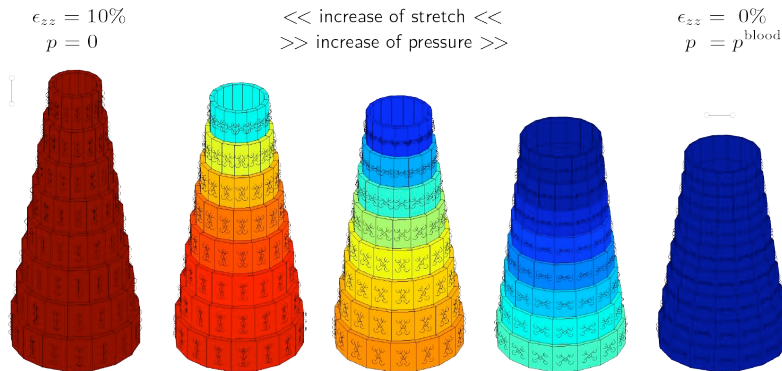
Kuhl & Holzapfel [2007]



example - arterial wall

36

sensitivity wrt pressure to stretch ratio



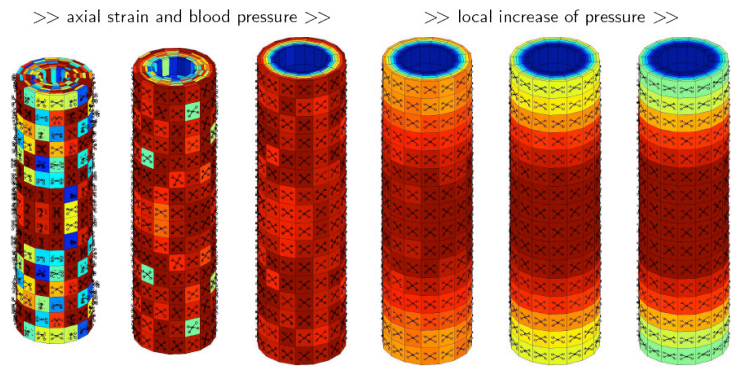
collagen fiber angle governed by pressure²stretch ratio

Kuhl & Holzapfel [2007]

example - arterial wall

37

sensitivity wrt changes in mechanical loading



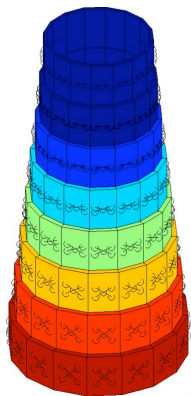
fiber reorientation in response to changes in loading

Kuhl & Holzapfel [2007]

example - arterial wall

38

hierarchical continuum model for living tissues

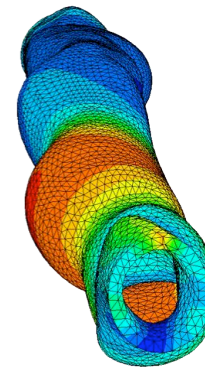


- fully three dimensional
orthotropy • transverse isotropy • isotropy
- micromechanically motivated
limited set of parameters $\lambda, \mu, L, A, \gamma^{\text{chn}}$
- non-affine chain network
 \mathbf{n}_I adapt instantaneously wrt eigenvectors $\mathbf{n}_I \doteq \mathbf{n}_I^\sigma$
 l_I adapt gradually wrt eigenvalues $l_I \rightarrow \lambda_I^{\sigma+} / \|\lambda_I^{\sigma+}\|$
- stress vs strain driven remodeling
eigenvectors commute • eigenvalues do not

remodeling

39

challenges - mechanotransduction



- how do tissues sense mechanical stimuli?
receptors on cell surface • cytoskeleton
- how are signals transmitted?
focal adhesion • role of biochemistry • ion channels
- how does remodeling take place?
collagen synthesis / turnover • gene expression

mechanics of the cell

remodeling

40